Digital Imaging

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Traditional Radiography

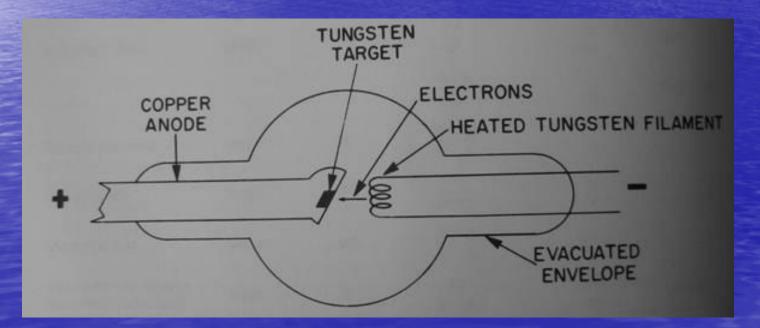
Production of x-rays
Beam restriction
Grids
Image recording
Film processing



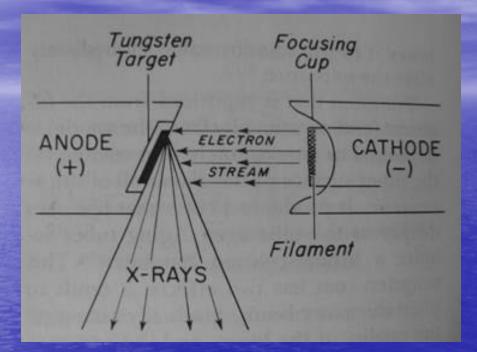


Production of x-rays

 Created by energy conversion within the TUBE
 The tube is made of pyrex glass and contains two electrodes in a vacuum. This is surrounded by oil and housed in a lead lined case



The x-ray tube



Electrons are created at the cathode (neg electrode/filament) by passing a current through the filament

They are accelerated toward the anode (pos electrode) where they will collide with the target

The cathode

• The x-ray tube current (mA) is the number of electrons flowing from the filament to the target per second The filament is made of tungsten The electrons leaving the filament are focused by a focusing cup usually made of nickel

The anode

- The target is a small plate of 90% tungsten, 10% rhenium embedded in a large piece of copper
- The electrons strike the target and produce xrays
- Only 1% of the energy of the electrons will become x-rays, 99% will result in heat
- Thus the anode rotates to facilitate heat dissipation into the copper

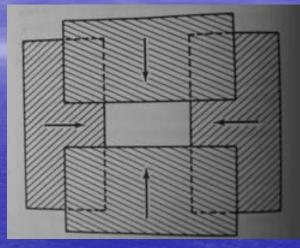
X-ray production

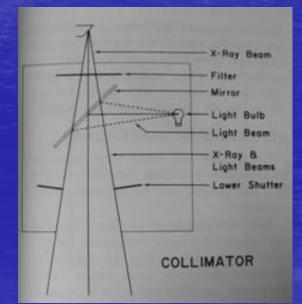
- The voltage difference created between the cathode and the anode (kVp) is responsible for the speed of the electrons
- X-rays are generated when electrons hit the target

The faster the electron, the more energy it has and the higher the energy of the x-ray it will generate

Beam restriction

- Collimator = two sets of shutters define the beam dimensions
- Infinite number of square or rectangular fields
- X-ray field visible as a lightened area



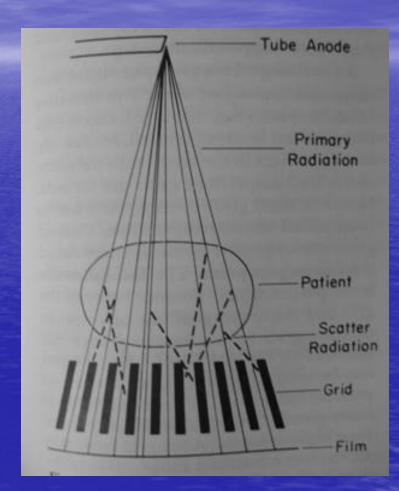


Pros of collimation

Limit the area exposed to the primary beam \rightarrow limit patient exposure \rightarrow limit the scatter that degrades the image \rightarrow and limit the scatter that interacts with personnel Win – Win maneuver Tricks for collimating rapidly

Grids

- Series of lead strips separated by radiolucent filler material
- Primary radiation is oriented in parallel with the strips and passes through untouched
- Scatter radiation is at off angles to the strips and is absorbed by them



Grid ratio = ratio of height of lead strips to distance between them Grids range between 4:1 and 16:1 (8:1) most commonly used) The higher the ratio the better the grid is at removing scatter but the more primary beam is necessary



Image recording

X-rays strike the cassette which contains fluorescent screens and the film Phosphors in the screen emit light within 10⁻⁸ seconds of stimulation by the x-ray (fluoresce) Light exposes the film Important that light sensitivity of the film matches that emitted by the phosphors

Intensifying screens

Decrease the x-ray dose to the patient (intensification factor)
Allow shorter exposure times – important to minimize motion blur
Original phosphor = crystalline calcium tungstate (produces blue light)

Screen speed

Faster screens (ie require less patient xray exposure to produce the same amount of x-ray film exposure) • Made faster by increasing thickness of phosphor layer Increased thickness decreases image clarity due to light diffusion

Newer phosphors: Rare earth

X-ray film

 Photographic emulsion attached to a supportive base

- Important emulsion components are gelatin and silver halide
- Gelatin holds silver halide grains evenly dispersed and is easily penetrated by processing solutions

Silver halide

Light sensitive material
90-99% silver bromide
1-10% silver iodide
Silver (Ag+), bromine (Br-) and iodine (I-) ions are arranged in a cubic lattice to form a crystal suspended in the gelatin

Latent image formation

Br- + light photon \rightarrow Br + electron

Electron moves within the crystal until it is trapped by a sensitivity speck (site of crystal imperfection)

Attracts silver ions

 $Ag+ + electron \rightarrow Ag$

Repeated trapping of electrons at the sensitivity speck causes the accumulation of silver

Clumps of silver = latent image centers

Film processing - developer

- Development will amplify the latent image by a factor of millions
- Developer is a reducing agent which changes the silver ion back to black metallic silver
- Reaction happens much more rapidly at latent image sites so time is important in development process

Replenishment

- Bromide and acid are formed and developer is consumed each time a film is developed
- Developer therefore needs to be replenished regularly and a has a limited lifetime
- In a busy practice a tank of developer will last from 2 to 3 months



 After development the image must be washed and then fixed

- Fixer removes silver halide not reduced to silver (not exposed → washed away)
- Fixing agent forms water soluble complexes with silver ions which are then washed away in the subsequent water bath
- Fixer also hardens the gelatin

The permanent image

 Assuming proper development, fixation and washing ...

Areas hit by light from x-ray exposure will be black (metallic silver) and non exposed areas will be white (silver halide washed out of emulsion)

How to make an image digital

- Digital camera
- Scanner
- Charge coupled devices (CCD)
- Computed radiography (CR)
- True digital or flat panel radiography (DR)



Digital Camera

- The image will be only as good as the original radiograph
- Eliminate all light except what is coming through the film
- Set camera on black and white, macro setting, highest resolution, NO flash
 Do not move

 Take one image of the entire film and another close up of suspect area. Move in close to the film to do this, don't use zoom.



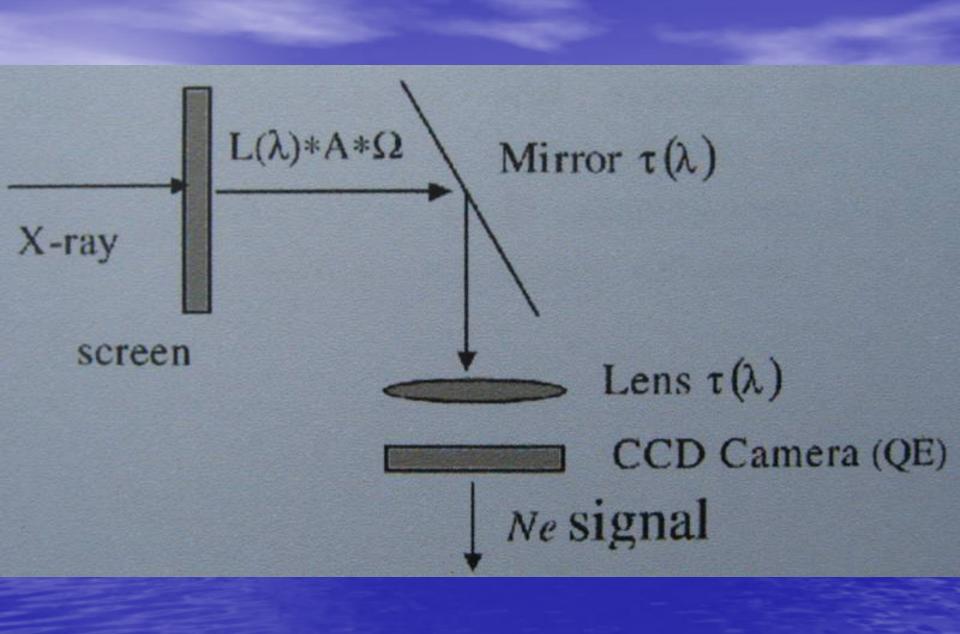


Good ones are very expensive!

Charge Coupled Devices (CCD)

 X-rays pass through patient and hit scintillator screen

Image created is projected by a mirror/lens assembly onto a CCD chip just as a camera focuses an image onto film
 CCD converts visible light into electrons that are stored in the CCD pixels



CCD

Consists of an integrated circuit containing an array of capacitors sensitive to light Each capacitor accumulates a charge proportional to the light intensity it sees The charge is then passed through an analog-to-digital converter Main uses are digital photography and astronomy

CCD concerns

CCDs are small relative to the scintillation screen – creates a lot of noise
Practical limit to the size of the CCD because of the time to read them out
Light loss through the lens assembly



The image

• Quality inferior to CR and DR • Noisy image with what looks like movement artifact Contrasty Not enough information stored for magnified images to be clear (grainy and blurry)

Computed Radiography

Traditional tube setup
Special cassette records image
Cassette manually placed in reader
Reader sends digital image to computer

The cassette

 Photostimulable phosphor that phosphoresces (emission of light after stimulation delayed beyond 10⁻⁸ seconds)

Preparing the plate for imaging

 Plate flooded with light from high intensity sodium discharge lamps → erases any previous image Photostimlable phosphor exposed to x-ray beam

- Some of energy of x-ray beam absorbed by phosphor
- Stored as valence electrons in high energy traps which forms the latent image
- Number of trapped electrons is proportional to the amount of x-rays absorbed
- Latent image will be retained for up to 8 hours but image will degrade over time

The reader

Laser beam scans latent image in cassette • Trapped electrons return to the valence band and emit light Photomultiplier tube records the light emission Photomultiplier tube output sent to computer where digital image is created

The reader

 Cassettes must be manually carried to and placed in reader





The image

 Of lesser to equal image quality as a traditional radiograph with screen

True digital imaging or flat panel imaging

Traditional tube setup
X-rays recorded by detector
Information sent immediately to computer

The detector

Stored permanently in your bucky tray
Direct wiring to computer image acquisition station
Near immediate appearance of image on the screen









The detector – Amorphous-Si/scintillator

- On top: x-ray scintillator made of thick layer of thallium-doped CsI or Gadolinium Oxide.
- Next: Array of amorphous silicon pin photodiodes and thin film transistors (TFT). Peak quantum efficiency of photodiodes = that of light emitted by scintillator
- Next: readout and drive electronics. Chips perform charge to voltage conversion.

The detector - Se

No scintillator intermediate, direct x-ray to electron conversion
Pass through Selenium photoconductor
Read by thin film transistors (TFT) detector elements

The detector

 Charge is collected by an integrating amplifier and converted to a voltage
 Programmable gain is applied to the signal voltage

 Output voltage is converted to digital data by analog-to-digital converter (ADC)
 This is performed row by row

The image

Excellent quality

 Images contain adequate information to magnify many times and still have great image



Pros and cons of digital radiography

Some true of all "digital" systems
Some vary by system chosen

Decreased costs

 No processor, processing space, processing solutions or maintenance No film expenses, film jackets or storage space needed No storage space for completed radiographs needed except computer No time spent filing new films or looking for old

Time investments

Taking radiographs

 Time to take films is same for traditional and CR – around 20-25 minutes a case. CR might be slightly faster as exposure latitude increased so retakes may be fewer

 Time with true DR or CCD drastically reduced to around a third of the time

Time Investments

Developing radiographs

 Regular processors around 1.5 minutes but films can go in one right after the other

 CR: takes around 1.5 minutes for image to be read and appear on computer, must wait for one to be completely done to go to next

 DR and CCD: Image appears on computer within seconds of exposure

Improvements – all systems

 Ability to see the image from any site within the hospital

Ability to manipulate the image: magnification, altering contrast/brightness
Ability to send (remote reads) or copy (for the client or referral) the exact image quickly

Improvements DR

 Exposures can be so close together that it will approximate fluoroscopy

Downside DR + CCD

 Mobile radiography is difficult due to the need for the cable attaching sensor and computer

 Cross table views cannot be obtained as the sensor is attached to the table

Downside to all - change

You will have to train personnel
 You likely will have to alter your technique chart

Downside - expense

Computed systems: 35 to 55 K
CCD: 45-70 K
Digital systems: 80 K and up
Number of workstations will cause the price to vary

Volume needed to consider a system

CR around 30 studies a month
CCD around 50
DR around 60 studies a month

Viewing stations

 Need very high resolution monitor to take advantage of image quality
 Grey scale vs color LCD



Imaging software and PACS systems

- Don't just need ability to produce the digital image
- Need software to view and manipulate the image
- Need to archive the image, retrieve the image, send the image, distribute the image throughout the hospital

PACS System - efficient storage and retrieval

P - Picture viewing at various workstations
A - Archiving images
C - Communication using LAN or internet
S - System



Immediate retrieval of all radiographs taken on a given patient
Storage and retrieval of any digital image generated on the patient (US, CT, MRI)
Off site backup by the PACS vendor or other independent image storage companies

 Access to images at the off site storage server by the client or referral hospitals

Image format

 Beware of vendor lock-in: Make sure images are not stored in a proprietary manner

 Common nonproprietary image formats: JPEG, JPEG200, TIFF, DICOM

DICOM – **Digital Imaging and Communications in Medicine** DICOM is an organization that concerns itself with the standardization of the communication of medical images and associated important information DICOM is a published standard with 18 different parts the goals of which are to "achieve compatibility and to improve workflow efficiency between imaging systems and other information systems in heathcare environments worldwide." DICOM is an imaging format.

DICOM image format

File format that permanently stores information about the date, patient and type of scan in the image header Require a DICOM viewer to view image DICOM image software should protect the image integrity and not allow you to alter the original image – it is part of the medical record

DICOM Standards

 Published and maintained by NEMA (National Equipment Manufacturers Association)

 A product should have a DICOM conformance statement that details what the product does and does not do relative to the DICOM standard

Not all parts are relevant to all products

Seven relevant parts for medical imaging

- Verification confirms is properly connected before communicating (pinging)
- Modality Worklist management scheduling communications
- Performed Procedure Step Communications about completed exams
- Store sending images to PACS
- Storage commit transfers ownership of images
 Print printing images
- Query/Retrieve exchange between display station and archive

Providers and users

 DICOM Store – Modality (eg CT) is user, PACS system is provider
 DICOM Query/Retrieve – PACS system is both provider (provides images to users) and user (uses images from storage)

DICOM specifications for a device

Tell you what class of service it supports
What role it plays (user, provider, both)
What objects (modalities) it supports

In summary – most important points to consider when shopping for a digital system Image quality most important Availability and dependability of service once installed – examine vendor's reputation closely • PACS system inclusion/availability DICOM compatibility Type of system: DR, CR, CCD – what are your goals and how much can you spend

